

1	Status	Final Text
2	Date of Last Update	2017/04/18
3	Person Assigned	David Clunie
4		mailto:dclunie@dclunie.com
5	Submitter Name	QIICR
6	Submission Date	2016/09/02

7	Correction Number CP-1665	
8	Log Summary: Add MR Diffusion Model Quantities and Parameters for Parametric Maps and ROI Measurements	
9	Name of Standard	
10	PS3.3, PS3.6, PS3.16, PS3.17 2017a	
11	Rationale for Correction:	
12	Appropriate codes exist to communicate in parametric maps and SR measurement reports that values are (G-C1C6, SRT, "Quantity")	
13	= (113041, DCM, "Apparent Diffusion Coefficient") and that the units are (mm ² /s, UCUM, "mm ² /s"), when a mono-exponential model	
14	characterized by a single value is used. Other diffusion models exist that produce other quantities than ADC (e.g., fast and slow	
15	compartment coefficients and their relative fraction for bi-exponential models)	
16	Further, the interpretation of the ADC and similar values may depend on the method of fitting and specific techniques used, as well	
17	as the b-values of the acquired images used as input.	
18	Accordingly, additional concepts are added for different quantities, methods and parameters, with examples of their use.	
19	Also, allow CT and MR Image and Frame Type Value 3 and Value 4 defined terms (as is already the case for Value 4 MR terms)	
20	for parametric maps (needed, if for no other reason, for consistency with the IHE DIFF profile to allow DIFFUSION for value 3).	
21	The choice of units for diffusion coefficients is also discussed.	
22	Other suggestions for models related to tractography that were received during the preparation of this CP will be deferred to a	
23	separate CP specific to those existing context groups.	
24	Correction Wording:	

Amend DICOM PS3.3 as follows (changes to existing text are bold and underlined for additions and ~~struckthrough~~ for removals):

C.7.6.16.2.11.1.2 Real World Values Mapping Sequence Attributes

The physical units for the real world values obtained from the sequence item are given by the Measurement Units Code Sequence (0040,08EA).

The quantity that the real world values represent may be described by the Quantity Definition Sequence (0040,9220), which consists of a list of name-value pairs, in which the coded concept name specifies what aspect of the physical quantity is being described.

Note

1. For example, Cerebral Blood Flow (CBF) may be described by units and quantity as follows:

- Measurement Units Code Sequence (0040,08EA) = (ml/[100]g/min, UCUM, "milliliter per 100 gram per minute")
- Quantity Definition Sequence (0040,9220):
 - (G-C1C6, SRT, "Quantity") = (113055, DCM, "Regional Cerebral Blood Flow")

2. For example, the Apparent Diffusion Coefficient (ADC) may be described by units and quantity as follows:

- Measurement Units Code Sequence (0040,08EA) = (mm²/s, UCUM, "mm²/s")
- Quantity Definition Sequence (0040,9220):
 - (G-C1C6, SRT, "Quantity") = (113041, DCM, "Apparent Diffusion Coefficient")

Additional information about how the ADC was derived, e.g., the model used, method of fitting and acquisition b-values used, can also be encoded as name-value pairs in the Quantity Definition Sequence (0040,9220). Other diffusion models and quantities are also defined. See the example in PS3.17 Annex EEEE.

The Quantity Definition Sequence (0040,9220) describes only the stored pixel values that are mapped using the Real World Values Mapping, and does not describe derived values from multiple pixels to which the Real World Values Mapping applies.

Note

I.e., the mapping is a "point" operation, and as a consequence various modifiers that might be applied to a group of pixels, such as in an ROI, should not be used. E.g., an ROI encoded in a Structured Report using TID 1419 "ROI Measurements" might be the mean or maximum value (e.g., SUVbw mean or SUVbw max), and be encoded with (121401, DCM, "Derivation") = (R-00317, SRT, "Mean") or (G-A437, SRT, "Maximum"), respectively. These would not be appropriate to use within Quantity Definition Sequence (0040,9220), unless the individual pixel values were themselves derived in such a manner, e.g., when multiple images are averaged together. Thus the content items used in an SR to describe an ROI might be a superset of the name-value pairs used in Quantity Definition Sequence (0040,9220).

C.8.32.2 Parametric Map Image Module

Table C.8.32-2. Parametric Map Image Module Attributes

Attribute Name	Tag	Type	Attribute Description
Image Type	(0008,0008)	1	Image identification characteristics. Enumerated Values for Value 1: DERIVED Enumerated Values for Value 2: PRIMARY Value 3 shall be Image Flavor, common Defined Terms for which are specified in Section C.8.16.1.3, CT-specific Defined Terms for which are specified in Section C.8.15.2.1.1.3 and MR-specific Defined Terms for which are specified in Section C.8.13.1.1.1.3. Value 4 shall be Derived Pixel Contrast, common Defined Terms for which are specified in Section C.8.16.1.4, CT-specific Defined Terms for which are specified in Section C.8.15.2.1.1.4 and MR-specific Defined Terms for which are specified in Section C.8.13.1.1.1.4.

C.8.32.3.1 Parametric Map Frame Type Macro

...

Table C.8.32-3. Parametric Map Frame Type Macro Attributes

Attribute Name	Tag	Type	Attribute Description
Parametric Map Frame Type Sequence	(0040,9092)	1	Identifies the characteristics of this Parametric Map frame. Only a single Item shall be included in this Sequence.
>Frame Type	(0008,9007)	1	Type of Frame. A multi-valued attribute analogous to Image Type (0008,0008). Enumerated Values and Defined Terms are the same as those for the four values of Image Type (0008,0008), except that the value MIXED is not allowed. See Section C.8.32.2.

Amend DICOM PS3.6 as follows (changes to existing text are bold and underlined for additions and ~~struckthrough~~ for removals):

A Registry of DICOM Unique Identifiers (UIDs) (Normative)**Table A-3. Context Group UID Values**

Context UID	Context Identifier	Context Group Name
<u>1.2.840.10008.6.1.1165</u>	CID 7270	MR Diffusion Component Semantics
<u>1.2.840.10008.6.1.1166</u>	CID 7271	MR Diffusion Anisotropy Indices
<u>1.2.840.10008.6.1.1167</u>	CID 7272	MR Diffusion Model Parameters
<u>1.2.840.10008.6.1.1168</u>	CID 7273	MR Diffusion Models
<u>1.2.840.10008.6.1.1169</u>	CID 7274	MR Diffusion Model Fitting Methods
<u>1.2.840.10008.6.1.1170</u>	CID 7275	MR Diffusion Model Specific Methods
<u>1.2.840.10008.6.1.1171</u>	CID 7276	MR Diffusion Model Inputs
<u>1.2.840.10008.6.1.1172</u>	CID 7277	Units of Diffusion Rate Area Over Time

Amend DICOM PS3.16 as follows (changes to existing text are bold and underlined for additions and ~~struckthrough~~ for removals):

CID 7180 Abstract Multi-dimensional Image Model Component Semantics

Type: Extensible
Version: ~~20160314~~20170413

Table CID 7180. Abstract Multi-dimensional Image Model Component Semantics

Coding Scheme Designator	Code Value	Code Meaning	SNOMED-CT Concept ID	UMLS Concept Unique ID
<i>Include CID 4033 "MR Proton Spectroscopy Metabolites"</i>				
DCM	113063	T1		
DCM	113065	T2		
DCM	113064	T2*		
DCM	113058	Proton Density		
DCM	110800	Spin Tagging Perfusion MR Signal Intensity		
DCM	113070	Velocity encoded		
DCM	113067	Temperature encoded		
DCM	110801	Contrast Agent Angio MR Signal Intensity		
DCM	110802	Time Of Flight Angio MR Signal Intensity		
DCM	110803	Proton Density Weighted MR Signal Intensity		
DCM	110804	T1 Weighted MR Signal Intensity		
DCM	110805	T2 Weighted MR Signal Intensity		
DCM	110806	T2* Weighted MR Signal Intensity		
<u>Include Section CID 7270 "MR Diffusion Component Semantics"</u>				
<u>Include Section CID 7271 "MR Diffusion Anisotropy Indices"</u>				
<u>Include Section CID 7272 "MR Diffusion Model Parameters"</u>				
DCM	413043	Diffusion-weighted		
DCM	110807	Field Map MR Signal Intensity		
DCM	410808	Fractional Anisotropy		
DCM	410809	Relative Anisotropy		
DCM	413044	Apparent Diffusion Coefficient		
DCM	410810	Volumetric Diffusion Dxx Component		
DCM	410811	Volumetric Diffusion Dxy Component		
DCM	410812	Volumetric Diffusion Dxz Component		
DCM	410813	Volumetric Diffusion Dyy Component		
DCM	410814	Volumetric Diffusion Dyz Component		
DCM	410815	Volumetric Diffusion Dzz Component		
DCM	110816	T1 Weighted Dynamic Contrast Enhanced MR Signal Intensity		
DCM	110817	T2 Weighted Dynamic Contrast Enhanced MR Signal Intensity		
DCM	110818	T2* Weighted Dynamic Contrast Enhanced MR Signal Intensity		

	Coding Scheme Designator	Code Value	Code Meaning	SNOMED-CT Concept ID	UMLS Concept Unique ID
1					
2					
3					
4	DCM	110819	Blood Oxygenation Level		
5	DCM	110820	Nuclear Medicine Projection Activity		
6	DCM	110821	Nuclear Medicine Tomographic Activity		
7	DCM	110822	Spatial Displacement X Component		
8	DCM	110823	Spatial Displacement Y Component		
9	DCM	110824	Spatial Displacement Z Component		
10	DCM	110825	Hemodynamic Resistance		
11	DCM	110826	Indexed Hemodynamic Resistance		
12	DCM	112031	Attenuation Coefficient		
13	DCM	110827	Tissue Velocity		
14	DCM	110828	Flow Velocity		
15	SRT	P0-02241	Power Doppler	425704008	C1960437
16	DCM	110829	Flow Variance		
17	DCM	110830	Elasticity		
18	DCM	110831	Perfusion		
19	DCM	110832	Speed of sound		
20	DCM	110833	Ultrasound Attenuation		
21	DCM	113068	Student's T-test		
22	DCM	113071	Z-score		
23	DCM	113057	R-Coefficient		
24	DCM	126220	R2-Coefficient		
25	DCM	110834	RGB R Component		
26	DCM	110835	RGB G Component		
27	DCM	110836	RGB B Component		
28	DCM	110837	YBR FULL Y Component		
29	DCM	110838	YBR FULL CB Component		
30	DCM	110839	YBR FULL CR Component		
31	DCM	110840	YBR PARTIAL Y Component		
32	DCM	110841	YBR PARTIAL CB Component		
33	DCM	110842	YBR PARTIAL CR Component		
34	DCM	110843	YBR ICT Y Component		
35	DCM	110844	YBR ICT CB Component		
36	DCM	110845	YBR ICT CR Component		
37	DCM	110846	YBR RCT Y Component		
38	DCM	110847	YBR RCT CB Component		
39	DCM	110848	YBR RCT CR Component		
40	DCM	110849	Echogenicity		
41	DCM	110850	X-Ray Attenuation		
42	DCM	112031	Attenuation Coefficient		
43	DCM	110852	MR signal intensity		

Coding Scheme Designator	Code Value	Code Meaning	SNOMED-CT Concept ID	UMLS Concept Unique ID
DCM	110853	Binary Segmentation		
DCM	110854	Fractional Probabilistic Segmentation		
DCM	110855	Fractional Occupancy Segmentation		
DCM	126393	R1		
DCM	126394	R2		
DCM	113098	Magnetization Transfer Ratio		
<i>Include CID 4107 "Tracer Kinetic Model Parameters"</i>				
<i>Include CID 4108 "Perfusion Model Parameters"</i>				
<i>Include CID 4109 "Model-Independent Dynamic Contrast Analysis Parameters"</i>				
DCM	126400	Standardized Uptake Value		
DCM	126401	SUVbw		
DCM	126402	SUVlbm		
DCM	126405	SUVlbm(Janma)		
DCM	126403	SUVbsa		
DCM	126404	SUVibw		

CID 7181 Abstract Multi-dimensional Image Model Component Units

Type: Extensible
Version: 2014111020170413

Table CID 7181. Abstract Multi-dimensional Image Model Component Units

Coding Scheme Designator	Code Value	Code Meaning
<i>Include CID 3500 "Pressure Units"</i>		
<i>Include CID 3502 "Hemodynamic Resistance Units"</i>		
<i>Include CID 3503 "Indexed Hemodynamic Resistance Units"</i>		
<i>Include CID 7460 "Units of Linear Measurement"</i>		
<i>Include CID 7461 "Units of Area Measurement"</i>		
<i>Include CID 7462 "Units of Volume Measurement"</i>		
<i>Include CID 84 "PET Units"</i>		
<i>Include CID 7277 "Units of Diffusion Rate Area Over Time"</i>		
UCUM	1	no units
UCUM	{ratio}	ratio
UCUM	[hnsfU]	Hounsfield Unit
UCUM	{counts}	Counts
UCUM	{counts}/s	Counts per second
UCUM	[arb'U]	arbitrary unit
UCUM	cm/s	centimeter/second
UCUM	mm/s	millimeter/second
UCUM	dB	decibel
UCUM	Cel	degrees Celsius

Coding Scheme Designator	Code Value	Code Meaning
UCUM	ml/min	milliliter per minute
UCUM	ml/s	milliliter per second
UCUM	ms	millisecond
UCUM	s	second
UCUM	Hz	Hertz
UCUM	mT	milliTesla
UCUM	{Particles}/[100]g{Tissue}	number particles per 100 gram of tissue
UCUM	mm2/s	square millimeter per second
UCUM	s/mm2	second per square millimeter
UCUM	ml/[100]g/min	milliliter per 100 gram per minute
UCUM	ml/[100]ml	milliliter per 100 milliliter
UCUM	mmol/kg{WetWeight}	millimoles per kg wet weight
UCUM	/min	/min
UCUM	/s	/s

Add new Context Groups to DICOM PS3.16 as follows:

CID 7270 MR Diffusion Component Semantics

Type: Extensible
Version: 20170413

Table CID 7270. MR Diffusion Component Semantics

Coding Scheme Designator	Code Value	Code Meaning	SNOMED-CT Concept ID	UMLS Concept Unique ID	Units
DCM	113043	Diffusion weighted			DT (1, UCUM, "no units")
DCM	110810	Volumetric Diffusion Dxx Component			DT (1, UCUM, "no units")
DCM	110811	Volumetric Diffusion Dxy Component			DT (1, UCUM, "no units")
DCM	110812	Volumetric Diffusion Dxz Component			DT (1, UCUM, "no units")
DCM	110813	Volumetric Diffusion Dyy Component			DT (1, UCUM, "no units")
DCM	110814	Volumetric Diffusion Dyz Component			DT (1, UCUM, "no units")
DCM	110815	Volumetric Diffusion Dzz Component			DT (1, UCUM, "no units")

CID 7271 MR Diffusion Anisotropy Indices

Type: Extensible
Version: 20170413

Table CID 7271. MR Diffusion Anisotropy Indices

Coding Scheme Designator	Code Value	Code Meaning	SNOMED-CT Concept ID	UMLS Concept Unique ID	Units
DCM	110808	Fractional Anisotropy			DT ({0:1}, UCUM, "range 0:1")
DCM	110809	Relative Anisotropy			DT ({ratio}, UCUM, "ratio")
DCM	113288	Volume Ratio			DT ({0:1}, UCUM, "range 0:1")

CID 7272 MR Diffusion Model Parameters

Type: Extensible
Version: 20170413

Table CID 7272. MR Diffusion Model Parameters

Coding Scheme Designator	Code Value	Code Meaning	SNOMED-CT Concept ID	UMLS Concept Unique ID	Units
DCM	113041	Apparent Diffusion Coefficient		C3890194	DCID 7277 "Units of Diffusion Rate Area Over Time"
DCM	113289	Diffusion Coefficient			DCID 7277 "Units of Diffusion Rate Area Over Time"
DCM	113290	Mono-exponential Apparent Diffusion Coefficient			DCID 7277 "Units of Diffusion Rate Area Over Time"
DCM	113291	Slow Diffusion Coefficient			DCID 7277 "Units of Diffusion Rate Area Over Time"
DCM	113292	Fast Diffusion Coefficient			DCID 7277 "Units of Diffusion Rate Area Over Time"
DCM	113293	Fast Diffusion Coefficient Fraction			DT ({0:1}, UCUM, "range 0:1")
DCM	113294	Kurtosis Diffusion Coefficient			DCID 7277 "Units of Diffusion Rate Area Over Time"
DCM	113295	Gamma Distribution Scale Parameter			DT (1, UCUM, "no units")
DCM	113296	Gamma Distribution Shape Parameter			DT (1, UCUM, "no units")
DCM	113297	Gamma Distribution Mode			DT (1, UCUM, "no units")
DCM	113298	Distributed Diffusion Coefficient			DCID 7277 "Units of Diffusion Rate Area Over Time"
DCM	113299	Anomalous Exponent Parameter			DT ({0:1}, UCUM, "range 0:1")

CID 7273 MR Diffusion Models

Type: Extensible
Version: 20170413

Table CID 7273. MR Diffusion Models

Coding Scheme Designator	Code Value	Code Meaning
DCM	113250	Mono-exponential diffusion model

Coding Scheme Designator	Code Value	Code Meaning
DCM	113251	Bi-exponential (IVIM) diffusion model
DCM	113252	Kurtosis diffusion model
DCM	113253	Gamma distribution model
DCM	113254	Stretched exponential diffusion model
DCM	113255	Truncated Gaussian diffusion model

Note

CID 7274 MR Diffusion Model Fitting Methods

Type: Extensible
Version: 20170413

Table CID 7274. MR Diffusion Model Fitting Methods

Coding Scheme Designator	Code Value	Code Meaning
DCM	113260	Log of ratio of two samples
DCM	113261	Least squares fit of multiple samples
DCM	113265	Levenberg–Marquardt
DCM	113266	Trust-Region
DCM	113267	Fixed-Dp
DCM	113268	Segmented-Unconstrained
DCM	113269	Segmented-Constrained
DCM	113270	Bayesian-Probability

Note

CID 7275 MR Diffusion Model Specific Methods

Type: Extensible
Version: 20170413

Table CID 7275. MR Diffusion Model Specific Methods

Coding Scheme Designator	Code Value	Code Meaning
DCM	113285	Voxelwise selection of b-value

Note

CID 7276 MR Diffusion Model Inputs

Type: Extensible
Version: 20170413

Table CID 7276. MR Diffusion Model Inputs

Coding Scheme Designator	Code Value	Code Meaning	Units
DCM	113240	Source image diffusion b-value	DT (s/mm ² , UCUM, "s/mm ² ")

Note

CID 7277 Units of Diffusion Rate Area Over Time

Type: Extensible
Version: 20170413

Table CID 7277. Units of Diffusion Rate Area Over Time

Coding Scheme Designator	Code Value	Code Meaning
UCUM	mm2/s	mm2/s
UCUM	um2/ms	um2/ms
UCUM	um2/s	um2/s
UCUM	10-6.mm2/s	10-6.mm2/s

Note

Amend DICOM PS3.16 as follows (changes to existing text are bold and underlined for additions and ~~struckthrough~~ for removals):

D DICOM Controlled Terminology Definitions (Normative)**Table D-1. DICOM Controlled Terminology Definitions**

Code Value	Code Meaning	Definition	Notes
110808	Fractional Anisotropy	Coefficient reflecting the fractional anisotropy of the tissues, derived from a diffusion weighted MR image. Fractional anisotropy is proportional to the square root of the variance of the Eigen values divided by the square root of the sum of the squares of the Eigen values.	<u>Basser PJ, Pierpaoli C. Microstructural and physiological features of tissues elucidated by quantitative-diffusion-tensor MRI. J Magn Reson B. 1996 Jun;111(3):209–19. http://citeseerx.ist.psu.edu/viewdoc/download?doi=10.1.1.162.2222&rep=rep1&type=pdf</u>
110809	Relative Anisotropy	Coefficient reflecting the relative anisotropy of the tissues, derived from a diffusion weighted MR image.	<u>Basser PJ, Pierpaoli C. Microstructural and physiological features of tissues elucidated by quantitative-diffusion-tensor MRI. J Magn Reson B. 1996 Jun;111(3):209–19. http://citeseerx.ist.psu.edu/viewdoc/download?doi=10.1.1.162.2222&rep=rep1&type=pdf</u>
110810	Volumetric Diffusion Dxx Component	Dxx Component of the diffusion tensor, quantifying the molecular mobility along the X axis.	
110811	Volumetric Diffusion Dxy Component	Dxy Component of the diffusion tensor, quantifying the correlation of molecular displacements in the X and Y directions.	
110812	Volumetric Diffusion Dxz Component	Dxz Component of the diffusion tensor, quantifying the correlation of molecular displacements in the X and Z directions.	
110813	Volumetric Diffusion Dyy Component	Dyy Component of the diffusion tensor, quantifying the molecular mobility along the Y axis.	

Code Value	Code Meaning	Definition	Notes
110814	Volumetric Diffusion Dyz Component	Dyz Component of the diffusion tensor, quantifying the correlation of molecular displacements in the Y and Z directions.	
110815	Volumetric Diffusion Dzz Component	Dzz Component of the diffusion tensor, quantifying the molecular mobility along the Z axis.	
113041	Apparent Diffusion Coefficient	<p>Values are derived by calculation of the apparent diffusion coefficient. <u>This concept may be used for the diffusion coefficient of various different models, e.g., mono-exponential (ADC_m), kurtosis (ADC_k), stretched-exponential (ADC_s).</u></p> <p><u>The "apparent" appellation is because the diffusion images from which the ADC is computed may also be affected by T2 contrast (T2 "shine-through"), so this concept is distinguished from a "pure" diffusion coefficient that is not so affected.</u></p>	<p><u>Graessner J. Frequently Asked Questions: Diffusion-Weighted Imaging (DWI). MAGNETOM Flash. Siemens. 2011 Jan. http://clinical-mri.com/wp-content/uploads/software_hardware_updates/Graessner.pdf</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm²: Correlation with Gleason score and repeatability of region of interest analysis. <i>Magnetic Resonance in Medicine</i>. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u></p>
121050	Equivalent Meaning of Concept Name	The human readable meaning of the name component of a name-value pair that is equivalent to the post-coordinated meaning conveyed by the coded name and its concept modifier children.	
121322	Source image for image processing operation	Image used as the source for an image processing operation.	
121401	Derivation	Method of deriving or calculating a measured value. E.g., mean, or maximum of set.	
126220	R2-Coefficient	Coefficient of determination, R ² . An indication of goodness of fit.	
...
<u>113240</u>	<u>Source image diffusion b-value</u>	<u>The diffusion sensitization factor (b value) used during acquisition of the source image used for a diffusion model.</u>	
<u>113241</u>	<u>Model fitting method</u>	<u>The method used to fit a set of data to a mathematical model. E.g., least squares.</u>	

Code Value	Code Meaning	Definition	Notes
113250	<u>Mono-exponential diffusion model</u>	<u>Mono-exponential (single compartment) Apparent Diffusion Coefficient (ADC) model.</u>	<p><u>Burdette JH, Elster AD, Ricci PE. Calculation of apparent diffusion coefficients (ADCs) in brain using two-point and six-point methods. J Comput Assist Tomogr. 1998 Oct;22(5):792-4. http://journals.lww.com/jcat/pages/articleviewer.aspx?year=1998&issue=09000&article=00023&type=abstract</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116-24. http://dx.doi.org/10.1002/mrm.25482</u></p>
113251	<u>Bi-exponential (IVIM) diffusion model</u>	<u>Bi-exponential intravoxel incoherent motion (IVIM) model.</u>	<p><u>Merisaari H, Movahedi P, Perez IM, Toivonen J, Pesola M, Taimen P, et al. Fitting methods for intravoxel incoherent motion imaging of prostate cancer on region of interest level: Repeatability and gleason score prediction. Magnetic Resonance in Medicine. 2016. http://dx.doi.org/10.1002/mrm.26169</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116-24. http://dx.doi.org/10.1002/mrm.25482</u></p> <p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175-84. http://dx.doi.org/10.1002/mrm.25765</u></p>
113252	<u>Kurtosis diffusion model</u>	<u>±</u>	<u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116-24. http://dx.doi.org/10.1002/mrm.25482</u>
113253	<u>Gamma distribution model</u>	<u>±</u>	<u>Oshio K, Shinmoto H, Mulkern RV. Interpretation of diffusion MR imaging data using a gamma distribution model. Magn Reson Med Sci. 2014;13: 191-195. http://dx.doi.org/10.2463/mrms.2014-0016</u>

Code Value	Code Meaning	Definition	Notes
113254	<u>Stretched exponential diffusion model</u>		<p><u>Bennett KM, Schmainda KM, Bennett RT, Rowe DB, Lu H, Hyde JS. Characterization of continuously distributed cortical water diffusion rates with a stretched-exponential model. Magn Reson Med. 2003;50: 727–734. http://dx.doi.org/10.1002/mrm.10581</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm²: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u></p>
113255	<u>Truncated Gaussian diffusion model</u>		<p><u>Yablonskiy DA, Bretthorst GL, Ackerman JJH. Statistical model for diffusion attenuated MR signal. Magnetic Resonance in Medicine. 2003;50(4):664–9. http://dx.doi.org/10.1002/mrm.10578</u></p>
113260	<u>Log of ratio of two samples</u>	<u>Model fitting by using the log of the ratio of the two samples.</u>	<p><u>Burdette JH, Elster AD, Ricci PE. Calculation of apparent diffusion coefficients (ADCs) in brain using two-point and six-point methods. J Comput Assist Tomogr. 1998 Oct;22(5):792–4. http://journals.lww.com/jcat/pages/articleviewer.aspx?year=1998&issue=09000&article=00023&type=abstract</u></p>
113261	<u>Least squares fit of multiple samples</u>	<u>Model fitting by least squares method from more than two samples.</u>	<p><u>Burdette JH, Elster AD, Ricci PE. Calculation of apparent diffusion coefficients (ADCs) in brain using two-point and six-point methods. J Comput Assist Tomogr. 1998 Oct;22(5):792–4. http://journals.lww.com/jcat/pages/articleviewer.aspx?year=1998&issue=09000&article=00023&type=abstract</u></p>
113265	<u>Levenberg–Marquardt</u>	<u>Model fitting by Levenberg–Marquardt method.</u>	<p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>
113266	<u>Trust-Region</u>	<u>Model fitting by Trust-Region method.</u>	<p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>
113267	<u>Fixed-Dp</u>	<u>Model fitting by Fixed-Dp method.</u>	<p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>
113268	<u>Segmented-Unconstrained</u>	<u>Model fitting by Segmented-Unconstrained method.</u>	<p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>
113269	<u>Segmented-Constrained</u>	<u>Model fitting by Segmented-Constrained method.</u>	<p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>

Code Value	Code Meaning	Definition	Notes
113270	<u>Bayesian-Probability</u>	<u>Model fitting by Bayesian-Probability method.</u>	<p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p> <p><u>Neil JJ, Bretthorst GL. On the use of bayesian probability theory for analysis of exponential decay date: An example taken from intravoxel incoherent motion experiments. Magnetic Resonance in Medicine. 1993;29(5):642–7. http://dx.doi.org/10.1002/mrm.1910290510</u></p>
...
113285	<u>Voxelwise selection of b-value</u>	<u>Diffusion modeling by voxelwise selection of b-values.</u>	<u>Gatidis S, Schmidt H, Martirosian P, Nikolaou K, Schwenzler NF. Apparent diffusion coefficient-dependent voxelwise computed diffusion-weighted imaging: An approach for improving SNR and reducing T2 shine-through effects. Journal of Magnetic Resonance Imaging. 2016;43(4):824–32. http://dx.doi.org/10.1002/jmri.25044</u>
113288	<u>Volume Ratio</u>	<u>Coefficient reflecting the anisotropy of the tissues, derived from a diffusion weighted MR image. It represents the volume of an ellipsoid whose semimajor axes are the three eigenvalues of the diffusion tensor divided by the volume of a sphere whose radius is the mean diffusivity.</u>	<u>Pierpaoli C, Basser PJ. Toward a quantitative assessment of diffusion anisotropy. Magn Reson Med. 1996 Dec 1;36(6):893–906. http://onlinelibrary.wiley.com/doi/10.1002/mrm.1910360612/abstract</u>
113289	<u>Diffusion Coefficient</u>	<u>The pure diffusion coefficient, i.e., one that is not affected by T2 contrast effects.</u>	<u>Graessner J. Frequently Asked Questions: Diffusion-Weighted Imaging (DWI). MAGNETOM Flash. Siemens. 2011 Jan. http://clinical-mri.com/wp-content/uploads/software_hardware_updates/Graessner.pdf</u>
113290	<u>Mono-exponential Apparent Diffusion Coefficient</u>	<u>The diffusion coefficient of a mono-exponential diffusion model (ADC_m).</u>	<u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström P.J, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm²: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u>

Code Value	Code Meaning	Definition	Notes
113291	Slow Diffusion Coefficient	The slow diffusion coefficient (D_s) of a bi-exponential intravoxel incoherent motion (IVIM) diffusion model.	<p><u>Merisaari H, Movahedi P, Perez IM, Toivonen J, Pesola M, Taimen P, et al. Fitting methods for intravoxel incoherent motion imaging of prostate cancer on region of interest level: Repeatability and gleason score prediction. Magnetic Resonance in Medicine. 2016. http://dx.doi.org/10.1002/mrm.26169</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u></p> <p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>
113292	Fast Diffusion Coefficient	The fast diffusion coefficient (D_f) of a bi-exponential intravoxel incoherent motion (IVIM) diffusion model.	<p><u>Merisaari H, Movahedi P, Perez IM, Toivonen J, Pesola M, Taimen P, et al. Fitting methods for intravoxel incoherent motion imaging of prostate cancer on region of interest level: Repeatability and gleason score prediction. Magnetic Resonance in Medicine. 2016. http://dx.doi.org/10.1002/mrm.26169</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u></p> <p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>

Code Value	Code Meaning	Definition	Notes
113293	<u>Fast Diffusion Coefficient Fraction</u>	<u>The fast diffusion fraction of a bi-exponential intravoxel incoherent motion (IVIM) diffusion model.</u>	<p><u>Merisaari H, Movahedi P, Perez IM, Toivonen J, Pesola M, Taimen P, et al. Fitting methods for intravoxel incoherent motion imaging of prostate cancer on region of interest level: Repeatability and gleason score prediction. Magnetic Resonance in Medicine. 2016. http://dx.doi.org/10.1002/mrm.26169</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström P.J, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u></p> <p><u>Barbieri S, Donati OF, Froehlich JM, Thoeny HC. Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs. Magnetic Resonance in Medicine. 2016;75(5):2175–84. http://dx.doi.org/10.1002/mrm.25765</u></p>
113294	<u>Kurtosis Diffusion Coefficient</u>	<u>The diffusion coefficient of a kurtosis diffusion model (ADC_k).</u>	<u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström P.J, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u>
113295	<u>Gamma Distribution Scale Parameter</u>	<u>The scale (theta) parameter of a gamma distribution diffusion model.</u>	<u>Oshio K, Shinmoto H, Mulkern RV. Interpretation of diffusion MR imaging data using a gamma distribution model. Magn Reson Med Sci. 2014;13: 191–195. http://dx.doi.org/10.2463/mrms.2014-0016</u>
113296	<u>Gamma Distribution Shape Parameter</u>	<u>The shape (k) parameter of a gamma distribution diffusion model.</u>	<u>Oshio K, Shinmoto H, Mulkern RV. Interpretation of diffusion MR imaging data using a gamma distribution model. Magn Reson Med Sci. 2014;13: 191–195. http://dx.doi.org/10.2463/mrms.2014-0016</u>
113297	<u>Gamma Distribution Mode</u>	<u>The mode (maximum value of probability density function) of a gamma distribution diffusion model. Computed as $(k-1)*theta$, for $k \geq 1$.</u>	<u>https://en.wikipedia.org/wiki/Gamma_distribution</u>
113298	<u>Distributed Diffusion Coefficient</u>	<u>The distributed diffusion coefficient of a stretched-exponential diffusion model (ADC_s).</u>	<p><u>Bennett KM, Schmainda KM, Bennett RT, Rowe DB, Lu H, Hyde JS. Characterization of continuously distributed cortical water diffusion rates with a stretched-exponential model. Magn Reson Med. 2003;50: 727–734. http://dx.doi.org/10.1002/mrm.10581</u></p> <p><u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström P.J, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u></p>

Code Value	Code Meaning	Definition	Notes
113299	Anomalous Exponent Parameter	The anomalous exponent (stretching, alpha) parameter of a stretched-exponential diffusion model. This describes the deviation of the signal attenuation from mono-exponential behavior	<u>Bennett KM, Schmainda KM, Bennett RT, Rowe DB, Lu H, Hyde JS. Characterization of continuously distributed cortical water diffusion rates with a stretched-exponential model. Magn Reson Med. 2003;50: 727–734. http://dx.doi.org/10.1002/mrm.10581</u> <u>Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, et al. Mathematical models for diffusion-weighted imaging of prostate cancer using b values up to 2000 s/mm2: Correlation with Gleason score and repeatability of region of interest analysis. Magnetic Resonance in Medicine. 2015;74(4):1116–24. http://dx.doi.org/10.1002/mrm.25482</u>

Add new Annex to DICOM PS3.17 as follows:

EEEE Encoding Diffusion Model Parameters for Parametric Maps and ROI Measurements (Informative)

This Annex contains examples of how to encode diffusion models and acquisition parameters within the Quantity Definition Sequence of Parametric Maps and in ROIs in Measurement Report SR Documents.

The approach suggested is to describe that an ADC value is being measured by using ADC (generic) as the concept name of the numeric measurement, and to add post-coordinated concept modifiers to describe:

- the model (e.g., mono-exponential, bi-exponential or other multi-compartment models) (drawn from CID 7273 "MR Diffusion Models")
- the method of fitting the data points to that model (e.g., for mono-exponential models, log of ratio of two samples, linear least-squares for log-intensities of all b-values) (drawn from CID 7274 "MR Diffusion Model Fitting Methods")
- relevant numeric parameters, such as the b-values used during acquisition of the source images (drawn from CID 7275 "MR Diffusion Model Specific Methods")

The model and method of fitting are encoded separately since even though the method of fitting is sometimes dependent on the model, the model may be known but not the method of fitting, or there may be no code for the method of fitting.

Note

1. The generic concept of ADC, (113041, DCM, "Apparent Diffusion Coefficient"), is used, rather than the specific concept of ADC_m, (113290, DCM, "Mono-exponential Apparent Diffusion Coefficient"), since the model is expressed in a post-coordinated manner. Most clinical users will not be concerned with which model was used, and so the ability to display and query for a single generic concept is preferred. However, model-specific pre-coordinated concepts for ADC are provided, as are concepts for other model parameters when a single ADC concept is inappropriate, e.g., for the fast and slow components of a bi-dimensional model.
2. The generic concept of (G-C306, SRT, "Measurement Method") is used to describe the model, rather than being used to describe the fitting method, since the model is the more important aspect of the measurement to distinguish. This pattern is consistent with historical precedent (e.g., in PS3.17 RRR.3 the model (Extended Tofts) for DCE-MR measurements is described using the Measurement Method and the fitting method is not described).

Also illustrated is how the (121050, DCM, "Equivalent Meaning of Concept Name") can be used to communicate a single human readable textual description for the entire concept.

EEEE.1 Encoding Diffusion Model Parameters for Parametric Maps

This example shows how to use the PS3.3 Table C.7.6.16-12b "Real World Value Mapping Item Macro Attributes" to describe pixel values of an ADC parametric map obtained from a pair of B0 and B1000 images using an EEEE fit to a mono-exponential function

(single compartment model). It elaborates on the simple example provided in PS3.3 Section C.7.6.16.2.11.1.2 by adding coded concepts that describe the model, the method of fitting and listing the b-values used.

- Real World Value Mapping Sequence (0040,9096)
 - ...
 - Real World Value Intercept (0040,9224) = "0"
 - Real World Value Slope (0040,9225) = "1E-06"
 - LUT Explanation (0028,3003) = "ADC mm2/s mono-exponential log ratio B0 and B1000"
 - LUT Label (0040,9210) = "ADC mm2/s"
 - Measurement Units Code Sequence (0040,08EA) = (mm2/s, UCUM, "mm2/s")
 - Quantity Definition Sequence (0040,9220):
 - CODE (G-C1C6, SRT, "Quantity") = (113041, DCM, "Apparent Diffusion Coefficient")
 - CODE (G-C306, SRT, "Measurement Method") = (113250, DCM, "Mono-exponential ADC model")
 - CODE (113241, DCM, "Model fitting method") = (113260, DCM, "Log of ratio of two samples")
 - NUMERIC (113240, DCM, "Source image diffusion b-value") = 0 (s/mm2, UCUM, "s/mm2")
 - NUMERIC (113240, DCM, "Source image diffusion b-value") = 1000 (s/mm2, UCUM, "s/mm2")
 - TEXT (121050, DCM, "Equivalent Meaning of Concept Name") = "ADC mono-exponential log ratio B0 and B1000"

In this usage, the text of the (121050, DCM, "Equivalent Meaning of Concept Name") is redundant with the value of LUT Explanation (0028,3003); either or both could be omitted.

The parameter describing a b-value of 0 is expected to be sent, and one should not assume that a b-value of 0 is used if it is absent, since some methods may use a low b-value (e.g., 50), which is not 0.

There is no consensus in the MR community or scientific literature as to the appropriate units to use to report diffusion coefficient values to the user, nor amongst the MR vendors as to how to encode them. In this example, the units are specified as "s/mm2". If the diffusion coefficient pixel values were encoded as integers with such a unit, they could then be encoded with a Rescale Slope of 1E-06, given the typical range of values encountered. Alternatively, the pixel values could be encoded as floating point pixel data values with identity rescaling. Or, if the units were specified "um2/s" (or "10-6.mm2/s", which is the same thing), then integer pixels could be used with a Rescale Slope of 1. Application software can of course rescale the values for display and convert the units as appropriate to the user's preference, as long as they are unambiguously encoded.

EEEE.2 Encoding Diffusion Model Parameters for ROIs in Measurement Report SR Documents

This example shows how to describe the mean ADC value of a region of interest on a volume of ADC values obtained from a pair of B0 and B1000 images fitting the log ratio of two samples to a mono-exponential function (single compartment model). In this case the template used is TID 1419 ROI Measurements.

- NUM (113041, DCM, "Apparent Diffusion Coefficient") = 0.75E-3 (mm2/s, UCUM, "mm2/s")
 - *HAS CONCEPT MOD CODE* (G-C306, SRT, "Measurement Method") = (113250, DCM, "Mono-exponential ADC model")
 - *HAS CONCEPT MOD CODE* (113241, DCM, "Model fitting method") = (113260, DCM, "Log of ratio of two samples")
 - *HAS CONCEPT MOD CODE* (121401, DCM, "Derivation") = (R-00317, SRT, "Mean")
 - *INFERRED FROM NUM* (113240, DCM, "Source image diffusion b-value") = 0 (s/mm2, UCUM, "s/mm2")
 - *INFERRED FROM NUM* (113240, DCM, "Source image diffusion b-value") = 1000 (s/mm2, UCUM, "s/mm2")

- 2 • *HAS CONCEPT MOD* TEXT (121050, DCM, "Equivalent Meaning of Concept Name") = "Mean ADC mono-exponential log ratio
- 3 B0 and B1000"

4 **EEEE.3 Relationship of Derived Diffusion Model Parametric Maps to Diffusion Weighted**

5 **Source Images**

6 This example illustrates how to describe the manner in which an ADC Parametric Map image was derived from B0 and B1000 images.
7 The intent is to provide links to the images, not to replicate all the information that can be provided in the Quantity Definition Sequence.

8 This particular example illustrates the reference from an ADC Parametric Map to a pair of Enhanced MR images, one for each b-value
9 (or a pair of subsets of frames of a single Enhanced MR image), but the same principle is applicable when single frame IODs are
10 used as source or derived image.

- 11 • Derivation Image Sequence (0008,9124)
 - 12 • Derivation Description (0008,2111) = "Calculation of mono-exponential ADC from log of ratio of B0 and B1000 images"
 - 13 • Derivation Code Sequence (0008,9215)
 - 14 • (113041, DCM, "Apparent Diffusion Coefficient")
 - 15 • (113250, DCM, "Mono-exponential ADC from log of ratio of two samples")
 - 16 • Source Image Sequence (0008,2112)
 - 17 • Item 1:
 - 18 • Referenced SOP Class UID (0008,1150) of B0 image
 - 19 • Referenced SOP Instance UID (0008,1155) of B0 image
 - 20 • Referenced Frame Number (0008,1160) of B0 frames in image
 - 21 • Purpose of Reference Code Sequence
 - 22 • (121322, DCM, "Source image for image processing operation")
 - 23 • Item 2:
 - 24 • Referenced SOP Class UID (0008,1150) of B1000 image
 - 25 • Referenced SOP Instance UID (0008,1155) of B1000 image
 - 26 • Referenced Frame Number (0008,1160) of B1000 frames in image
 - 27 • Purpose of Reference Code Sequence
 - 28 • (121322, DCM, "Source image for image processing operation")

29 In this approach:

- 30 • since multiple items are permitted in the Derivation Code Sequence (0008,9215), both the general concept (calculation of ADC)
- 31 and the specific method have been listed; alternatively, just one or the other could be provided
- 32 • a textual description has also be provided, which in this case provides more information than the structured content (i.e., about the
- 33 b-values used)
- 34 • a generic purpose of reference code has been used, since only a single code is permitted and there is no mechanism (other than
- 35 creating pre-coordinated codes for every possible b-value) to convey which image (set) was acquired with which b-value; the more
- 36 specific alternative of a coded concept for "source image for ADC calculation" would add no value over the concept already described
- 37 in Derivation Code Sequence

- the SOP Instance UID in the first and second items may be the same, but a different range of frames referenced, e.g., if all of the source frames (all of the b-values) are in the same instance, as is required by the IHE Diffusion (DIFF) profile (http://wiki.ihe.net/index.php/MR_Diffusion_Imaging); if all of the frames in a single source image are used, then only a single item is necessary and the Referenced Frame Number can be omitted.
- all of the images have been listed in a single item of Derivation Image Sequence (0008,9124); alternatively, multiple items of Derivation Image Sequence (0008,9124) could be sent, one for each of the different b-values used; this would allow Derivation Description (0008,2111) to communicate which set contained which b-value, but there is no structured way to communicate such numeric parameters (other than creating pre-coordinated codes for every possible b-value)

EEEE.4 Image and Frame of Derived Diffusion Model Parametric Maps

This example illustrates how to encode the Image and Frame Type values of an ADC Parametric Map image.

Parametric maps are of the enhanced multi-frame family, so they use the standard roles of Image Flavor for Value 3 and Derived Pixel Contrast for Value 4.

The specific requirements are defined in PS3.3 Section C.8.32.2 "Parametric Map Image Module" and PS3.3 Section C.8.32.3.1 Parametric Map Frame Type Macro.

Since this is a derived diffusion image that contains ADC value, suitable values are:

- Image Type (0008,0008) = "DERIVED\PRIMARY\DIFFUSION\ADC"

This usage is consistent with the requirements for Image and Frame Type in the IHE Diffusion (DIFF) profile (http://wiki.ihe.net/index.php/MR_Diffusion_Imaging).

EEEE.5 Informative References

This section lists useful references related to the taxonomy of ADC calculation methods.

EEEE.5.1 ADC Method Descriptions

[Burdette 1998] *J Comput Assist Tomogr*. Burdette JH, Elster AD, and Ricci PE. 1998. 22. 5. 792–4. "Calculation of apparent diffusion coefficients (ADCs) in brain using two-point and six-point methods". <http://journals.lww.com/jcat/pages/articleviewer.aspx?year=1998&issue=09000&article=00023&type=abstract> .

[Barbieri 2016] *Magnetic Resonance in Medicine*. Barbieri S, Donati OF, Froehlich JM, and Thoeny HC. 2016. 75. 5. 2175–84. "Impact of the calculation algorithm on biexponential fitting of diffusion-weighted MRI in upper abdominal organs". <http://dx.doi.org/10.1002/mrm.25765> .

[Bennett 2003] *Magnetic Resonance in Medicine*. Bennett KM, Schmainda KM, Bennett RT, Rowe DB, Lu H, and Hyde JS. 2003. 50. 727–734. "Characterization of continuously distributed cortical water diffusion rates with a stretched-exponential model". <http://dx.doi.org/10.1002/mrm.10581> .

[Gatidis 2016] *Journal of Magnetic Resonance Imaging*. Gatidis S, Schmidt H, Martirosian P, Nikolaou K, and Schwenzer NF. 2016. 43. 4. 824–32. "Apparent diffusion coefficient-dependent voxelwise computed diffusion-weighted imaging: An approach for improving SNR and reducing T2 shine-through effects". <http://dx.doi.org/10.1002/jmri.25044> .

[Graessner 2011] *MAGNETOM Flash*. Graessner J. 2011. 84-87. "Frequently Asked Questions: Diffusion-Weighted Imaging (DWI)". Siemens Healthcare. http://clinical-mri.com/wp-content/uploads/software_hardware_updates/Graessner.pdf .

[Merisaari 2016] *Magnetic Resonance in Medicine*. Merisaari H, Movahedi P, Perez IM, Toivonen J, Pesola M, Taimen P, Boström PJ, Pahikkala T, Kiviniemi A, Aronen HJ, and Jambor I. 2016. "Fitting methods for intravoxel incoherent motion imaging of prostate cancer on region of interest level: Repeatability and gleason score prediction". <http://dx.doi.org/10.1002/mrm.26169> .

[Neil 1993] *Magnetic Resonance in Medicine*. Neil JJ and Bretthorst GL. 1993. 29. 5. 642–7. "On the use of bayesian probability theory for analysis of exponential decay date: An example taken from intravoxel incoherent motion experiments". <http://dx.doi.org/10.1002/mrm.1910290510> .

- 1 [Oshio 2014] *Magn Reson Med Sci*. Oshio K, Shinmoto H, and Mulkern RV. 2014. 13. 191–195. “Interpretation of diffusion MR imaging
2 data using a gamma distribution model”. <http://dx.doi.org/10.2463/mrms.2014-0016> .
- 3 [Toivonen 2015] *Magnetic Resonance in Medicine*. Toivonen J, Merisaari H, Pesola M, Taimen P, Boström PJ, Pahikkala T, Aronen
4 HJ, and Jambor I. 2015. 74. 4. 1116–24. “Mathematical models for diffusion-weighted imaging of prostate cancer using b
5 values up to 2000 s/mm²: Correlation with Gleason score and repeatability of region of interest analysis”. [http://dx.doi.org/
6 10.1002/mrm.25482](http://dx.doi.org/10.1002/mrm.25482) .
- 7 [Yablonskiy 2003] *Magnetic Resonance in Medicine*. Yablonskiy DA, Bretthorst GL, and Ackerman JJH. 2003. 50. 4. 664–9. “Statist-
8 ical model for diffusion attenuated MR signal”. <http://dx.doi.org/10.1002/mrm.10578> .